

Inverse and control problems with applications to cancer detection and therapy

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Dedicated to Prof. L.A. Medeiros on his 90th birthday

- 1 Background (I): Inverse problems
- 2 Elastography
 - A geometric inverse problem
 - A Calderon-like problem
- 3 Background (II): Control problems
- 4 Therapy strategies
 - An optimal control problem oriented to therapy
 - A controllability problem and an open question
- 5 Additional results and comments

Some words on **inverse problems**:

- General setting of a **direct** problem:
Data ($\mathcal{D}_0 \cup \mathcal{D}_1$) \rightarrow **Results** (\mathcal{R}) \rightarrow **Observation (additional information)** (\mathcal{I})
- A related inverse problem:
Some data (\mathcal{D}_0) + **Information** (\mathcal{I}) \rightarrow **The other data** (\mathcal{D}_1)

Main questions for **the inverse problem**:

- **Uniqueness**: $\mathcal{I} = \mathcal{I}' \Rightarrow \mathcal{D}_1 = \mathcal{D}'_1$?
- **Stability**: Estimate $\text{dist}(\mathcal{D}_1, \mathcal{D}'_1)$ in terms of $\text{dist}(\mathcal{I}, \mathcal{I}')$
- **Reconstruction**: Compute (exact or approximately) \mathcal{D}_1 from \mathcal{I}

FIRST IP: identification of the **shape** of a domain

(a) Direct problem:

Data: Ω , φ and D

Result: the solution u to

$$(1) \quad \begin{cases} -\Delta u = 0, & x \in \Omega \setminus \overline{D} \\ u = 0, & x \in \partial D; \quad u = \varphi, & x \in \partial\Omega \end{cases}$$

Information:

$$(2) \quad \frac{\partial u}{\partial n} = \alpha, \quad x \in \gamma \subset \partial\Omega$$

(b) Inverse problem:

(Partial) data: Ω and φ

(Additional) information: α (on γ)

Goal: Find D such that the solution to (1) satisfies (2)

[Andrieux-et-al 1993], [Alessandrini-et-al 2000 . . .], [Kavian 2002],
[Alvarez-et-al 2005], [Dobova-EFC-GlezBurgos-Ortega 2006],
[Yan-Ma 2008]

Some general ideas

A first IP: solid detection

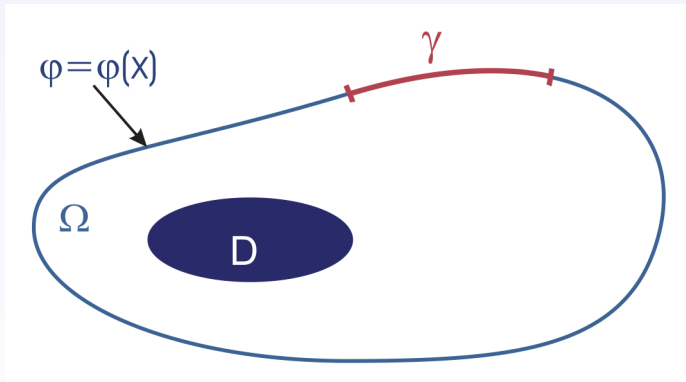


Figure: A geometrical inverse problem: identification of the open set D from Ω , φ and the additional information $\frac{\partial u}{\partial \nu} = \sigma$ on γ

SECOND IP: identification of the **conductivity** of a dielectric body (Calderón)

(a) Direct problem:

Data: Ω , φ and $a = a(x)$

Result: the solution u to

$$(1) \quad \begin{cases} -\nabla \cdot (a(x) \nabla u) = 0, & x \in \Omega \\ u = \varphi, & x \in \partial\Omega \end{cases}$$

Information:

$$(2) \quad u|_{\omega} = z$$

(b) Inverse problem:

(Partial) data: Ω and φ

(Additional) information: z (in ω)

Goal: Find a such that the solution to (1) satisfies (2)

Applications to tomography ...

[Calderón 1980], [Sylvester-Uhlman 1987], [Astala-Paavarinta 2003], ...

We consider: IPs of these kinds for the Lamé system

$$u_{tt} - \mu \Delta u - (\lambda + \mu) \nabla(\nabla \cdot u) = 0 \\ + \dots$$

$u = (u_1, \dots, u_N)$ is the field of displacements
 λ, μ are the Lamé coefficients (measure of stiffness)

We assume isotropic homogeneous media and small displacements

Elastography:

A technique to detect **elastic properties of tissue**

Aspects:

- Three elements: **Acoustic waves generator**, **Captor**, **Mathematical solver** (MR or ultrasound, identification of tissue stiffness)
- **Medical fields of application**: breast, liver, prostate and other cancers; arteriosclerosis, fibrosis, deep vein thrombosis, ...
- At present: emerging techniques (a very precise description)

First works: [Ophir-et-al 1991], [Muthupillai-et-al 1995], [Sinkus-et-al 2000], [McKnight-et-al 2002], ...

Many interesting problems in Medicine, Biology, etc. lead to IPs for PDEs of this class: **coefficient, source or shape identification**

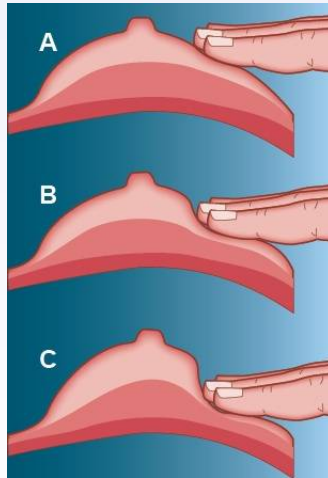


Figure: Classical detection methods in mammography (I): palpation

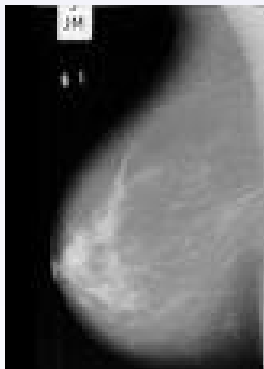


Figure: Classical detection methods in mammography (II): x-rays

Elastography is better suited than palpation and x-rays techniques:

- Tumors can be far from the surface
- or small
- or may have properties indistinguishable through palpation or x-rays

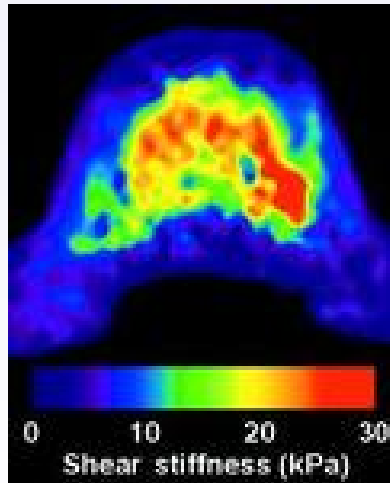


Figure: A breast elastogram. Identification of tissue stiffness

FIRST IP PROBLEM:

a **solid** tumor (D) inside an **elastic** tissue region (Ω)

The known data: Ω , T , (u_0, u_1) , μ , λ , φ

The system:

$$\begin{cases} u_{tt} - \mu \Delta u - (\lambda + \mu) \nabla(\nabla \cdot u) = 0 & \text{in } \Omega \setminus \overline{D} \times (0, T) \\ u = \varphi & \text{on } \partial\Omega \times (0, T) \\ u = 0 & \text{on } \partial D \times (0, T) \\ u(x, 0) = u_0(x), \quad u_t(x, 0) = u_1(x) & \text{in } \Omega \setminus \overline{D} \end{cases}$$

The observation: $\sigma(u) \cdot n := (\mu(\nabla u + \nabla u^T) + \lambda(\nabla \cdot u)\text{Id.}) \cdot n$ on $\gamma \times (0, T)$

The unknown: D

Uniqueness? Reconstruction algorithms and results?

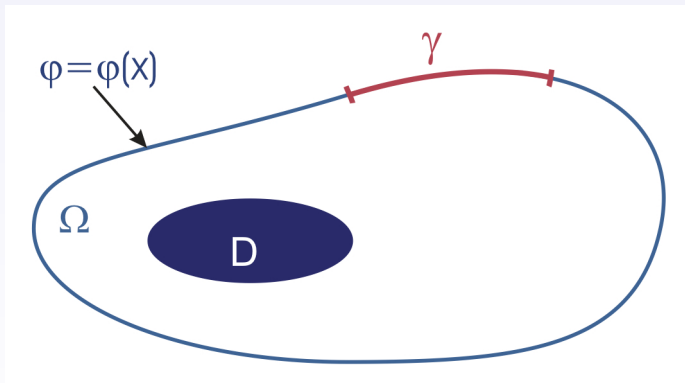


Figure: A geometrical inverse problem: identification of the open set D from Ω , φ and the additional information $\frac{\partial u}{\partial \nu} = \sigma$ on γ

UNIQUENESS

For $i = 0, 1$:

$$\begin{cases} u_{tt}^i - \mu \Delta u^i - (\lambda + \mu) \nabla (\nabla \cdot u^i) = 0 & \text{in } \Omega \setminus \overline{D^i} \times (0, T) \\ u^i = \varphi & \text{on } \partial\Omega \times (0, T) \\ u^i = 0 & \text{on } \partial D^i \times (0, T) \\ u^i(x, 0) = u_0(x), \quad u_t^i(x, 0) = u_1(x) & \text{in } \Omega \setminus \overline{D^i} \end{cases}$$

Two observations: $\alpha^i = \sigma(u^i) \cdot n$ on $\gamma \times (0, T)$

Theorem [Uniqueness]

Assume $D^0, D^1 \subset\subset \Omega$ non-empty and convex, $T > T_*(\Omega, \gamma)$

Then $\alpha^0 = \alpha^1 \Rightarrow D^0 = D^1$

The key point in the proof: **a unique continuation property**

(For $\mu = \mu(x)$ and/or $\lambda = \lambda(x)$ other uniqueness results can be applied:
Escauriaza, 2005; Nakamura-Wang, 2006; Imanuvilov-Yamamoto, 2012, ...)

RECONSTRUCTION

The usual technique: solve a related extremal problem

The case of a ball

$\tilde{\alpha} = \tilde{\alpha}(x, t)$ is given

Find x_0 and r such that $(x_0, r) \in X_b$

$$J(x_0, r) \leq J(x'_0, r') \quad \forall (x'_0, r') \in X_b, \quad (x_0, r) \in X_b$$

Here:

$$X_b := \{ (x_0, r) \in \mathbb{R}^4 : \overline{B}(x_0; r) \subset \Omega, r > 0 \}$$

$$J(x_0, r) := \frac{1}{2} \iint_{\gamma \times (0, T)} |\alpha[x_0, r] - \tilde{\alpha}|^2 ds dt$$

$$\alpha[x_0, r] := \sigma(u) \cdot n \text{ on } \gamma \times (0, T)$$

The difficulties: 3D, lack of sensitivity

The algorithm: Augmented Lagrangian + DIRECTNoScal

- Augmented Lagrangian \rightarrow a sequence of extremal problems with **only side constraints**
- DIRECTNoScal: a variant of the DIRECT algorithm, a **dividing rectangle** strategy

$$u_{01} = 10x, \quad u_{02} = 10y, \quad u_{03} = 10z$$

Test: $T = 5$, $u_{11} = 0$, $u_{12} = 0$, $u_{13} = 0$

$$\varphi_1 = 10x, \quad \varphi_2 = 10y, \quad \varphi_3 = 10z$$

$$x_{0des} = -2, \quad y_{0des} = -2, \quad z_{0des} = -2, \quad r_{des} = 1$$

$$x_{0ini} = 0, \quad y_{0ini} = 0, \quad z_{0des} = 0, \quad r_{ini} = 0.6$$

NLopt (AUGLAG + DIRECTNoScal), N° Iter = 1005, FreeFem++:

-2.139917695 -2.469135802 -2.713001067 0.8166666667

$$x_{0cal} = -1.981405274$$

$$y_{0cal} = -2.225232904$$

$$z_{0cal} = -2.148084171$$

$$r_{cal} = 0.9504115226$$

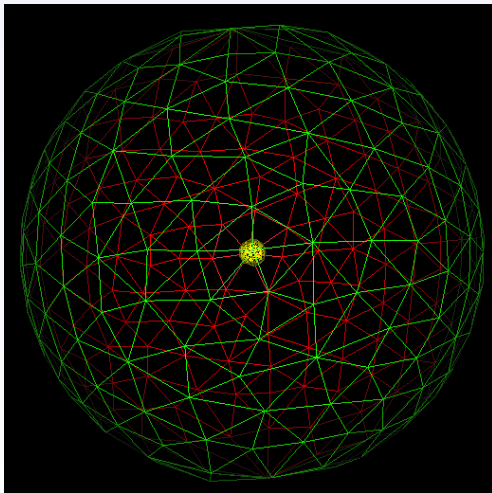


Figure: Initial mesh. Points: 829, tetrahedra: 4023, faces: 8406, edges: 5210, boundary faces: 720, boundary edges: 1080

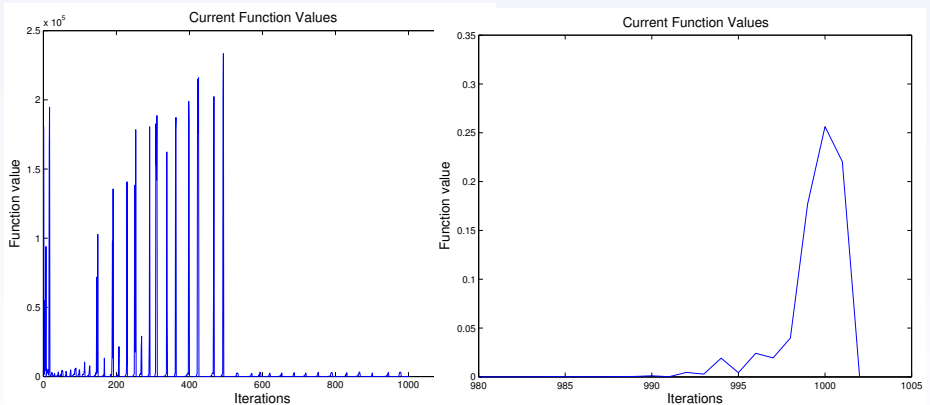


Figure: Cost evolution versus number of iterates (left) and detail (right).

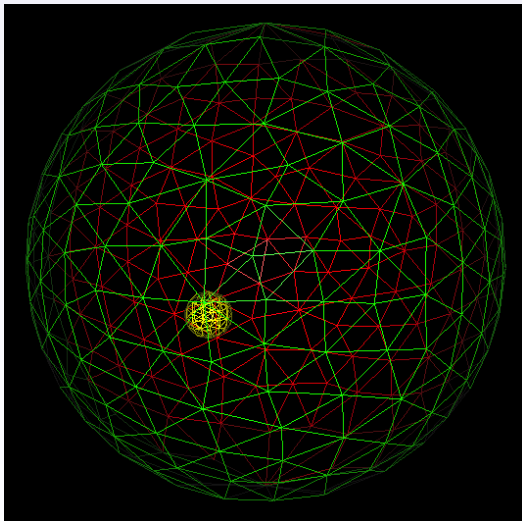


Figure: Desired and computed configuration

SECOND IP PROBLEM:

the tumor is **elastic** (very different μ and λ)

The known data: Ω , T , (u_0, u_1) , φ

The system:

$$\begin{cases} u_{tt} - \nabla \cdot (\mu(\nabla u + \nabla u^T) + \lambda(\nabla \cdot u)\text{Id.}) = f(x, t) & \text{in } \Omega \times (0, T) \\ u = \varphi & \text{on } \partial\Omega \times (0, T) \\ u(x, 0) = u_0(x), \quad u_t(x, 0) = u_1(x) & \text{in } \Omega \end{cases}$$

The observation: $\sigma(u) \cdot n := (\mu(\nabla u + \nabla u^T) + \lambda(\nabla \cdot u)\text{Id.}) \cdot n$ on $\gamma \times (0, T)$

The unknowns: $\mu = \mu(x)$ and $\lambda = \lambda(x)$

More difficult – **Reconstruction** algorithms and results?

RECONSTRUCTION

Assume $f, f_t \in L^2(Q)^N$, $u_0 = 0$, $u_1 \in H_0^1(\Omega)^N$, $\Upsilon \in L^2(\Sigma)^N$

Introduce a related (direct) extremal problem ($R > 0$ is given):

$$\begin{cases} \text{Minimize } I(\mu, \lambda) \\ \text{Subject to } (\mu, \lambda) \in \mathbb{K}(R) \end{cases}$$

$$I(\mu, \lambda) := \frac{1}{2} \int_0^T \|\sigma(u) \cdot n|_\gamma - \Upsilon\|^2 dt$$

$$\mathbb{K}(R) = \{ (\mu, \lambda) \in \mathbb{BV}(\Omega), \alpha \leq \mu, \lambda \leq \beta, TV(\mu), TV(\lambda) \leq R \}$$

Theorem

For all $R > 0$ there exists at least one solution (μ_R, λ_R) .

Idea the proof:

- A minimizing sequence (μ_n, λ_n) converges **weakly-*** in $\mathbb{BV}(\Omega)$, **strongly** in $L^p(\Omega)$ for all $p < +\infty$
- The associated $(u_n, u_{n,t}, u_{n,tt})$ converge **weakly-***
- $\nabla u_n \in$ **compact set in $L^2(Q)$** (much more in fact!) – A delicate point
Implied by **Meyers' estimates** together with **interpolation** results, [Tartar]

A NUMERICAL EXPERIMENT, FIXED λ

The domain and the mesh

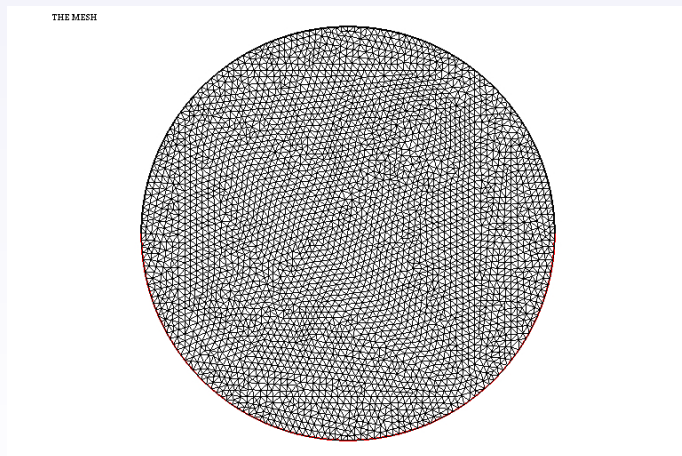


Figure: Number of nodes: 3629 – Number of triangles: 7056

TEST 1

Starting: $\mu = 5$ Target: $\mu = 10$ in D , $\mu = 1$ outside

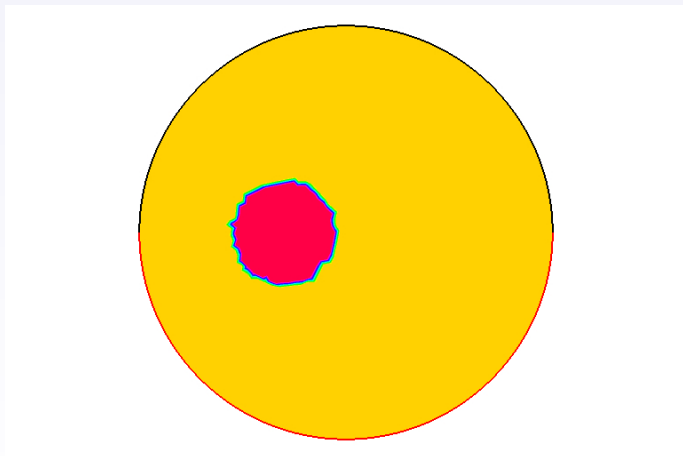


Figure: The target μ

The algorithm: Augmented Lagrangian + L-BFGS
(limited memory quasi-Newton, Broyden, Fletcher, Goldfarb and Shanno)
Final cost $\sim 9.6 \times 10^{-8}$, 158 comp. of the cost, 78 comp. of the gradient.

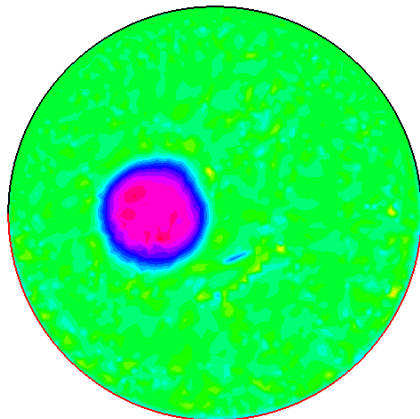


Figure: The computed μ

TEST 2

Starting: $\mu = 5$ Target: $\mu = 10$ in $D_1 \cup D_2$, $\mu = 1$ outside

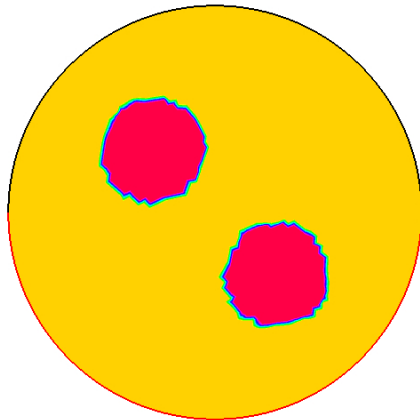


Figure: The target μ

The algorithm: Augmented Lagrangian + L-BFGS

Final cost $\sim 9.6 \times 10^{-8}$, 180 comp. of the cost, 80 comp. of the gradient.

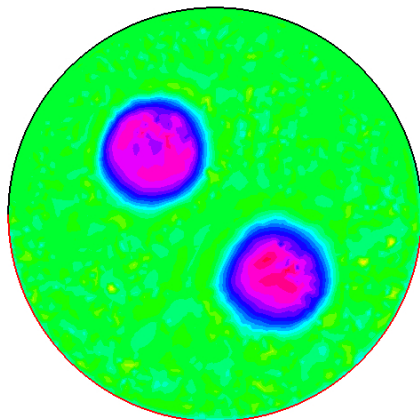


Figure: The computed μ

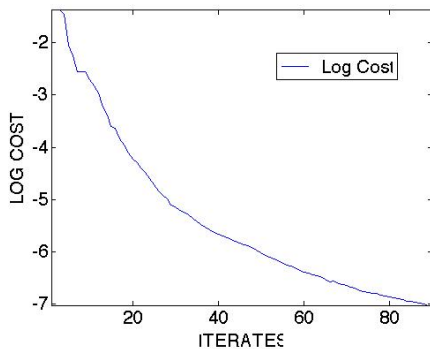
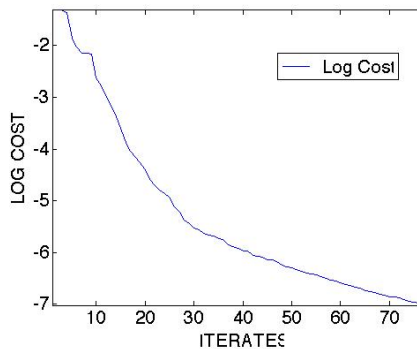


Figure: log of the cost versus number of iterates. Case 1 (left) and Case 2 (right).

CONTROL PROBLEMS

What is usual: act to get good (or the best) results for

$$\begin{cases} E(\textcolor{red}{U}) = F \\ + \dots \end{cases}$$

What is easier? **Solving?** **Controlling?**

Two classical approaches:

- Optimal control
- Controllability

OPTIMAL CONTROL

A general optimal control problem

Minimize $J(\mathbf{v})$

Subject to $\mathbf{v} \in \mathcal{V}_{ad}$, $\mathbf{y} \in \mathcal{Y}_{ad}$, (\mathbf{v}, \mathbf{y}) satisfies

$$E(\mathbf{y}) = F(\mathbf{v}) + \dots \quad (S)$$

Main questions: \exists , uniqueness/multiplicity, characterization, computation, ...

We could also consider similar bi-objective optimal control:

$$\begin{cases} \text{"Minimize"} & J_1(\mathbf{v}), J_2(\mathbf{v}) \\ \text{Subject to} & \mathbf{v} \in \mathcal{V}_{ad}, \dots \end{cases}$$

A lot of contributions: [Pontryaguin, J.-L. Lions, Kunisch, Troltsch, ...]

CONTROLLABILITY

A null controllability problem

Find (v, y)

Such that $v \in \mathcal{V}_{ad}$, (v, y) satisfies (ES), $y(T) = 0$

with $y : [0, T] \mapsto H$,

$$E(y) \equiv y_t + A(y) = F(v) + \dots \quad (ES)$$

Again many interesting questions: \exists , uniqueness/multiplicity, characterization, computation, ...

A very rich subject for PDEs, see [Russell, J.-L. Lions, Coron, Zuazua, ...]

A general tumor growth model

$$\begin{cases} y_t + Ay = B(y, v) \\ + \dots \end{cases}$$

$y = (y_1, \dots, y_n)$ is (for instance) a n -tuple of cell densities

$v = (v_1, \dots, v_m)$ is the therapy strategy (a radiation, a drug, a surgery, ...)

Very usually: $B(\cdot, \cdot)$ is bilinear!

We may ask v either

- To maximize a benefit (optimal control)
- Or lead y to a desired state (controllability)

AN OPTIMAL CONTROL PROBLEM

A) *Pre-therapy*:

$$\left\{ \begin{array}{ll} C_{0,t} &= D\Delta C_0 + \rho(1 - C_0) C_0, & \text{in } Q_0 := \Omega \times (0, t_1), \\ C_0(x, 0) &= c_0(x), & x \in \Omega, \\ \frac{\partial C_0}{\partial \nu} &= 0, & \text{on } \Sigma_0 := \partial\Omega \times (0, t_1). \end{array} \right. \quad (1)$$

B) *j-th therapy* for $j = 1, 2, \dots, n-1$:

$$\left\{ \begin{array}{ll} C_{j,t} &= D\Delta C_j + \rho(1 - C_j) C_j, & \text{in } Q_j := \Omega \times (t_j, t_{j+1}), \\ C_j(x, t_j) &= S(d_j(x))C_{j-1}(x, t_j), & x \in \Omega, \dots \end{array} \right. \quad (2)$$

Here: $S(d_j) := e^{-\alpha_t d_j - \beta_t d_j^2}$

C) *Post-therapy*:

$$\left\{ \begin{array}{ll} C_{n,t} &= D\Delta C_n + \rho(1 - C_n) C_n, & \text{in } Q_n := \Omega \times (t_n, +\infty), \\ C_n(x, t_n) &= S(d_n(x))C_{n-1}(x, t_n), & x \in \Omega, \dots \end{array} \right. \quad (3)$$

The state: (C_0, C_1, \dots, C_n) (normalized cell densities, $0 \leq C_j \leq 1$)

The control: $(t_1, \dots, t_n; d_1, \dots, d_n)$

AN OPTIMAL CONTROL PROBLEM

Maximize

$$T_*(t_1, \dots, t_n; d_1, \dots, d_n) := \inf \{ T \in \mathbb{R}_+ : \int_{\Omega} C(x, T^+) dx > M_* \}$$

Subject to $(t_1, \dots, t_n; d_1, \dots, d_n) \in \mathcal{U}_{ad}$

$$\begin{aligned} \mathcal{U}_{ad} \quad &:= \{ (t_1, \dots, t_n; d_1, \dots, d_n) \in \mathbb{R}^n \times L^2(\Omega)^n : \\ &0 \leq t_1 \leq \dots \leq t_n \leq \tilde{T}, \quad 0 \leq d_j \leq d_* \text{ a.e.}, \\ &\alpha_t \sum_{j=1}^n d_j + \beta_t \sum_{j=1}^n |d_j|^2 \leq E_* \text{ a.e.} \}, \end{aligned}$$

Difficulties:

- Bilinear action of the control, acting on initial data at each t_j (instantaneous, Dirac)
- Possibly nonregular functional

Optimal control oriented to therapy

Maximizing survival times with radiotherapy actions

Illustration of the process:

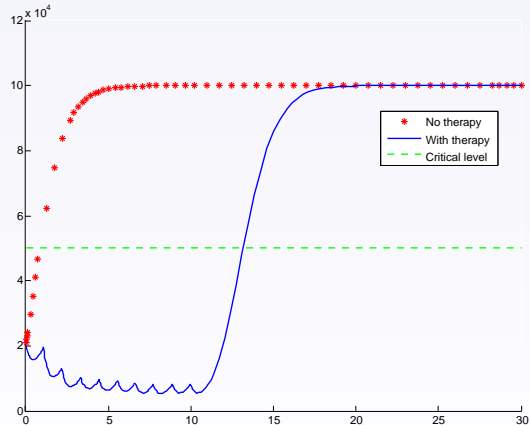


Figure: What we expect to get ...

Maximize

$$T_*(t_1, \dots, t_n; d_1, \dots, d_n) := \inf \{ T \in \mathbb{R}_+ : \int_{\Omega} C(x, T^+) dx > M_* \}$$

Subject to $(t_1, \dots, t_n; d_1, \dots, d_n) \in \mathcal{U}_{ad}$

An existence result:

Theorem [existence of optimal control]

Assume: $0 < M_* < |\Omega|$. Then: there exists at least one optimal control.

Idea of the proof:

- $\forall (t_1, \dots, t_n; d_1, \dots, d_n) \in \mathcal{U}_{ad} : \{ T : \int_{\Omega} C(x, T^+) dx > M_* \} \neq \emptyset$
and $T_*(t_1, \dots, t_n; d_1, \dots, d_n)$ makes sense
- \mathcal{U}_{ad} is bounded, closed and convex
- $(t_1, \dots, t_n; d_1, \dots, d_n) \mapsto T_*(t_1, \dots, t_n; d_1, \dots, d_n)$ is u.s.c.

Hence, ...

A numerical experiment in a simplified but realistic situation:

Fixed times t_j , free and constant d_j ; $n = 40$

<i>Monday</i>	<i>Tuesday</i>	<i>Wednesday</i>	<i>Thursday</i>	<i>Friday</i>	<i>Sat</i>	<i>Sun</i>
.	.	X	X	X	.	.
X	X	X	X	X	.	.
X	X	X	X	X	.	.
X	X	X	X	X	.	.
X	X	X	X	X	.	.
X	X	X	X	X	.	.
X	X	X	X	X	.	.
X	X	X	X	X	.	.
X	X

Table: Treatment with 40 doses in 8 weeks.

A numerical experiment in a simplified but realistic situation:

Cycle	4 weeks	5 weeks	6 weeks	7 weeks	8 weeks
C-dose	179.085	195.752	209.945	226.501	243.050
SQP	179.086*	195.752*	209.945*	226.502*	243.050*
AS	179.010	195.750	209.945	226.499	243.048
IP	178.983	195.666	209.866	226.418	243.047

Table: Comparisons of the computed survival times for various cycle durations. "C-dose" means all $d_j = d_{st.}$; "SQP" means *sequential quadratic programming* algorithm; "AS" means *active-set* algorithm; "IP" means *interior point* algorithm.

A numerical experiment in a simplified but realistic situation:

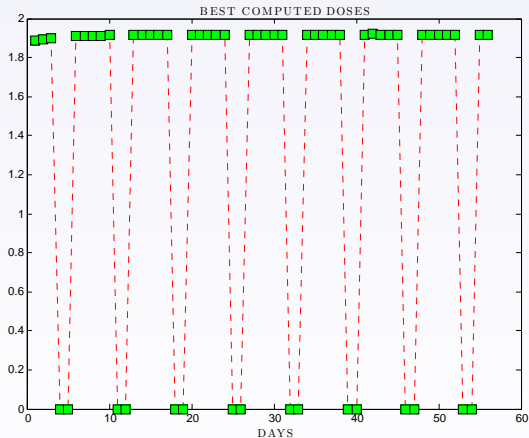


Figure: The best 40 doses found with the SQP algorithm (quasi-constant distribution).

A numerical experiment in a simplified but realistic situation:

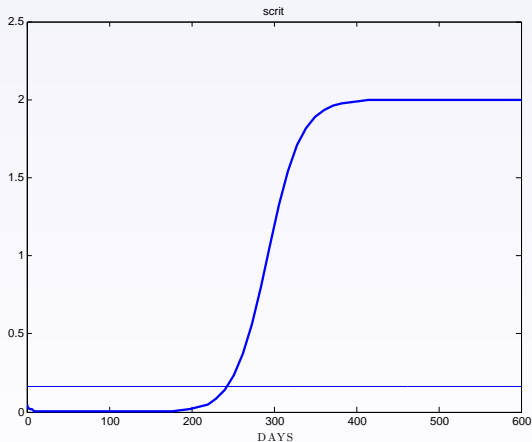


Figure: Evolution in time of the tumor size – 40 doses.

A numerical experiment in a simplified but realistic situation:

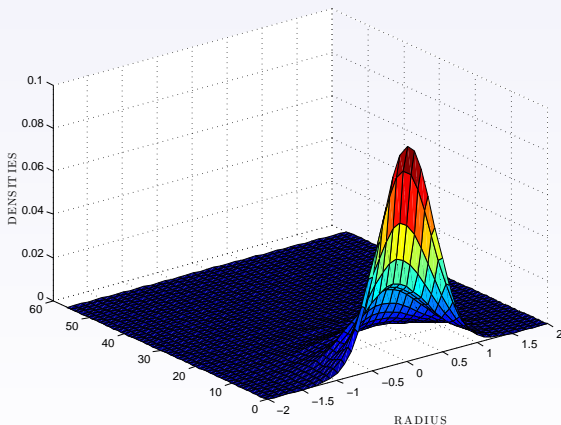


Figure: The evolution in time of the density of tumor cells (3D views) – 40 doses; pre-therapy and therapy.

A numerical experiment in a simplified but realistic situation:

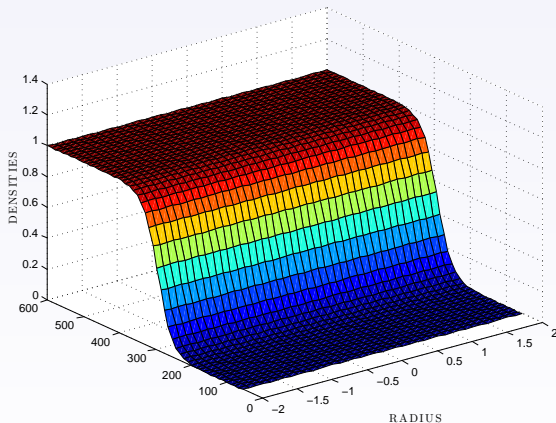


Figure: The evolution in time of the density of tumor cells (3D views) – 40 doses; post-therapy.

A numerical experiment in a simplified but realistic situation:

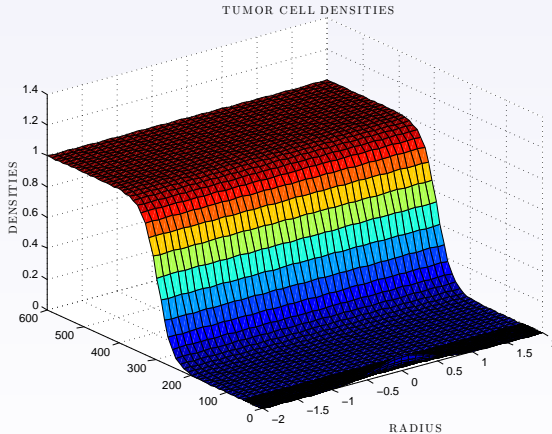


Figure: The evolution in time of the density of tumor cells (3D views) – 40 doses; global evolution.

Exact controllability to the trajectories oriented to therapy

Cell populations determined by radiotherapy actions

AN EXACT CONTROLLABILITY PROBLEM

An idealized model:

$$\begin{cases} c_t - \Delta c = (\mathbf{v}1_\omega)c, & (x, t) \in Q \\ c(x, 0) = c_0(x), & x \in \Omega, \dots \end{cases}$$

c : the cancer cell population \mathbf{v} : the radiotherapy action

The exact controllability problem: Find \mathbf{v} such that $c(x, T) \equiv \bar{c}(x, T)$
(\bar{c} is a fixed solution, another cell population)

Reformulation as a null controllability problem: $c = \bar{c} + y$, $c_0 = \bar{c}(\cdot, 0) + y_0$

$$\begin{cases} y_t - \Delta y = (\mathbf{v}1_\omega)(\bar{c} + y), & (x, t) \in Q \\ y(x, 0) = y_0(x), & x \in \Omega, \dots \end{cases}$$

The goal is now: Find \mathbf{v} such that $y(x, T) \equiv 0$

For interesting applications:

$$\bar{c}(\cdot, 0), c_0 \geq 0, \quad \bar{c}(\cdot, 0), c_0 \not\equiv 0, \quad y_0 = c_0 - \bar{c}(\cdot, 0) \geq 0 \quad (\text{large})$$

Exact controllability to the trajectories oriented to therapy

Cell populations determined by radiotherapy actions

What we pretend:

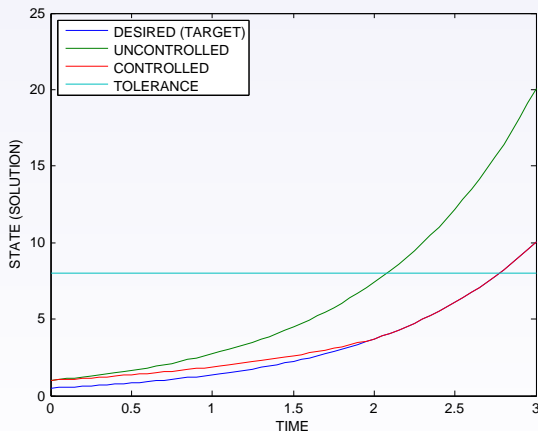


Figure: The desired, the uncontrolled and the controlled trajectories.

Exact controllability to the trajectories oriented to therapy

Cell populations determined by radiotherapy actions

$$\begin{cases} y_t - \Delta y = (v 1_\omega)(\bar{c} + y), & (x, t) \in Q \\ y(x, 0) = y_0(x), & x \in \Omega, \dots \end{cases}$$

Goal: Find v such that $y(x, T) \equiv 0$

Note: we can assume that $\bar{c} \geq 2\delta > 0$ in $\omega \times (0, T)$

A local result:

Theorem [Local controllability; Khapalov, 1990's]

$\exists \varepsilon > 0$ such that $y_0 \geq 0, \|y_0\|_{L^2} \leq \varepsilon \Rightarrow \text{OK}$

For the proof, solve the NC problem for

$$\begin{cases} y_t - \Delta y = u 1_\omega, & (x, t) \in Q \\ y(x, 0) = y_0(x), & x \in \Omega, \dots \end{cases}$$

Then take $v := u/(\bar{c} + y)$ in $\omega \times (0, T)$

y_0 small $\Rightarrow u$ small $\Rightarrow y \geq -\delta$ in $\omega \times (0, T) \Rightarrow \bar{c} + y \geq \delta$ in $\omega \times (0, T)$

Exact controllability to the trajectories oriented to therapy

Cell populations determined by radiotherapy actions

$$\begin{cases} y_t - \Delta y = (v1_\omega)(\bar{c} + y), & (x, t) \in Q \\ y(x, 0) = y_0(x), & x \in \Omega, \dots \end{cases}$$

Goal: Find v such that $y(x, T) \equiv 0$

An open problem: NC for large y_0 ?

It would suffice: global approximate controllability, i.e.

For small $\varepsilon > 0$, find v_ε such that $\|y(\cdot, T)\|_{L^2} \leq \varepsilon$

Unknown

A related question:

$$\begin{cases} y_t - \Delta y = u1_\omega, & (x, t) \in Q \\ y(x, 0) = y_0(x), & x \in \Omega, \dots \end{cases}$$

For small $\varepsilon > 0$, $\delta > 0$, find $u_{\varepsilon, \delta}$ such that

$$\|y(\cdot, T)\|_{L^2} \leq \varepsilon, \quad y \geq -\delta \text{ in } \omega \times (0, T)$$

Also unknown – Note: false for $\delta = 0$!

IN PROGRESS:

- Calderón-like IPs for 3D Lamé systems, with F. Mestre
- Radiotherapy optimal strategies for more complex systems, with L. Prouvée
- Optimal chemotherapy techniques for spherical tumors, with M. Cavalcanti and A.L. Ferreira

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THANK YOU VERY MUCH ...

AND CONGRATULATIONS TO PROF. LUIS ADAUTO !!! ...